# CT SCANNER PERFORMANCE EVALUATION

# **GREEN LIGHT IMAGING, LLC**

Medical Mobile Diagnostics 8348 Rosemead Blvd Pico Rivera, CA 90660

(562)222-1321

# CT Trailer #4

GE Optima CT520 Gantry S/N: 377671HM3

Survey Date: September 23, 2024

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#### CT SCANNER PERFORMANCE EVALUATION SUMMARY Site: GREEN LIGHT IMAGING, LLC Report Date: September 27, 2024 8348 Rosemead Blvd Survey Date: September 23, 2024 Pico Rivera, CA 90660 Model: Optima CT520 X-Ray Unit Manufacturer: General Electric Medical Systems July 1, 2014 CT Trailer #4 **Date Manufactured:** Room ID: Khachig A. Jerjian, Ph.D. **Medical Physicist:** Signature: PASS/FAIL/NA **Review of Clinical CT Protocols PASS** 1. 2. **PASS** Scout Prescription Accuracy Evaluation 3. Laser Light Alignment Accuracy Evaluation **PASS** 4. **Table Travel Accuracy Evaluation PASS** 5. Radiation Beam Width Accuracy Evaluation **PASS**

6.

7.

8.

Slice Thickness Accuracy Evaluation

Low Contrast Performance Evaluation

**High Contrast Spatial Resolution Evaluation** 

**PASS** 

**PASS** 

**PASS** 

## **MEDICAL PHYSICS RECOMMENDATIONS & COMMENTS**

- 1. CT scanner performance evaluation was found to be adequate. Performance evaluation test results were within ACR recommended action limits. Deviations in the indicated and measured  $\text{CTDI}_{\text{vol}}$  dose values were within the acceptable range of  $\pm$  20%.
- 2. Select clinical protocols for adult and pediatric patients were reviewed. Protocols were found to be adequate with typical doses within ACR recommended Reference Dose Levels for both head and body protocols.
- 3. Brain Perfusion CT protocols were not reviewed. Brain CT Perfusions are not performed on this scanner.
- 4. CT number calibration dependence on kVp and Slice Thickness was found to be adequate for all kVp stations. CT Number linearity and contrast scale were also found to be adequate.
- 5. Technologist QC program is well established. Daily QC procedures are properly performed and documented on the days of scanner use. Recommend documenting the monthly visual checklist and display monitor QC tests also.
- 6. Detailed accounts of this performance evaluation may be obtained by contacting us directly at (949)683-5215 or by e-mail at kjmedicalphysics@gmail.com.

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Date: September 27, 2024

# 1. REVIEW OF ROUTINE CLINICAL CT PROTOCOLS

This CT scanner performance evaluation was performed using the ACR CT Accreditation Program Phantom and routine clinical head and abdomen protocols used at this facility. Test procedures were consistent with ACR CT Accreditation Program guidelines.

Table 1. Routine Protocols

For this continue techniques used on an appropriate or appropriate	Adult	Adult	Pediatric	Pediatric
For this section, techniques used on an average patient or average technique calculated from several patient images is recorded.	Head	Abdomen	Head	Abdomen
			(1 Year Old)	(5 Year Old)
kVp	120	120	100	100
mA	150	275	190	200
Time per Rotation (sec)	2.0	1.0	0.8	0.8
System Calculated mAs	300	275	152	160
Effective mAs (or mAs per slice) as displayed	300	200	152	116
Scan FOV (cm)	Head(25 cm)	Large(50 cm)	Ped(25 cm)	Small(25 cm)
Display FOV (cm)	25 cm	36 cm	25 cm	25 cm
Reconstruction Algorithm	Stnd	Stnd Plus	Standard	Std Plus
Axial (A) or Helical (H) Scan	Α	Н	Α	Н
Acquisition Slice Thickness Z-Axis Collimation (T in				
mm)	1.25	1.25	1.25	1.25
Number of Slices per Tube Rotation - # of Data				
Channels Used (N)	16	16	16	16
Table Increment (mm) (axial scans) or Table Speed				
(mm/rot)(helical scans) (I)	20.0	27.5	20.0	27.5
IEC definition of Pitch for this protocol				
(Pitch = I / N * T) (calculated by the System)	1.0	1.375	1.0	1.375
Reconstructed Scan Width (mm)	5.0	2.5	5.0	2.5
Reconstructed Scan Interval (mm)	5.0	2.5	5.0	2.5
Dose Reduction Technique(s) used in routine		Auto mA 75-	Auto mA	Auto mA 50-
patient scanning for these protocols ( <i>Note: The</i>		350 mA Noise	50-190 mA	200 mA Noise
ACR and CTDI phantoms are NOT scanned with		Index 15.86	Noise Index	Index 12.69
dose reduction options. )		1=00	1.41	10.00
Indicated CTDIvol (mGy)	51.29 mGy	17.26 mGy	17.24 mGy	13.33 mGy
Reference Dose Phantom Size	Head 16	Body 32	Head 16	Head 16

The facility clinical protocol acquisition and reconstruction parameters were reviewed for specific requirements of the diagnostic imaging task, adequate image quality and dose. The above listed protocols were found to be adequate. The High Resolution Chest protocol was also found to be adequate. Brain Perfusion protocols were not reviewed. Brain Perfusions are not performed on this scanner.

## 2. SCOUT PRESCRIPTION ACCURACY EVALUATION

**Phantom:** ACR CT Accreditation Phantom

**Technique:** 120 kVp, 200 mA, 0.8 sec Rotation Speed, 160 mAs, Axial Mode, 2x0.625 mm Detector

Configuration, 1.25 mm Slice Thickness, Bone Reconstruction Algorithm, Large SFOV, 21 cm

DFOV, 512x512 Image Matrix.

Following proper position and leveling of the phantom on the scan table at the center of the gantry and acquisition of scout images, 1.25 mm thick axial images were prescribed at the center of modules 1 and 4 of the ACR CT Accreditation phantom at table landmark position of +0 mm and at table location 120 mm superior to the landmark position. Slice localization from scout prescription accuracy was evaluated using images of embedded 1 mm diameter BBs at the surface of modules 1 and 4 of the ACR phantom.

Detector Configuration	Nominal Position	Nominal Position Actual Location Deviation (	
1i 2x0.625 mm	Landmark Location	0.0 mm	0.0 mm
	Superior +120 mm	+120.0 mm	0.0 mm

**Conclusion:** Slice localization from scanned projection radiographs/scout was found to be adequate, accurate

to within ± 1 mm.

## 3. LASER LIGHT ALIGNMENT ACCURACY EVALUATION

<b>Detector Configuration</b>	Nominal Position	Actual Location	Deviation (mm)
1i 2x0.625 mm	Landmark Location	0.0 mm	0.0 mm
	Azimuth 0° Laser	Left/Right	0.0 mm
	Azimuth 90° & 270°	Vertical	0.0 mm

• Maximum discrepancy between the internal and external axial laser lights and the plane of radiation field was determined to be less than ± 1 mm. The sagital and coronal laser light alignment accuracy was also found to be adequate, within ± 2 mm limits.

**Conclusion:** Bed positioning accuracy and congruence of the laser light beam localizer with the imaging plane

was found to be adequate.

## 4. TABLE TRAVEL ACCURACY EVALUATION

Detector Configuration	Nominal Position	Actual Location	Deviation (mm)	
1i 2x0.625 mm	Landmark Location	0.0 mm	0.0 mm	
	Superior +120 mm	+120.0 mm	0.0 mm	

• Maximum discrepancy in bed repositioning was determined to be less than ± 1 mm.

**Conclusion:** CT scanner table motion was accurate, reproducible and consistent with digital system indicators.

Bed travel and indexing/incrementation accuracy was found to be adequate and reproducible to

within ±1 mm.

# 5. BEAM WIDTH ACCURACY EVALUATION

**Phantom:** CR Plate

**Technique:** 80 kVp, 10 mA, 0.8 sec Rotation Speed, 8 mAs, Axial Mode, Detector Configuration and Slice

Thicknesses as indicated, Standard Reconstruction Algorithm, Large SFOV, 40 cm DFOV,

512x512 Image Matrix.

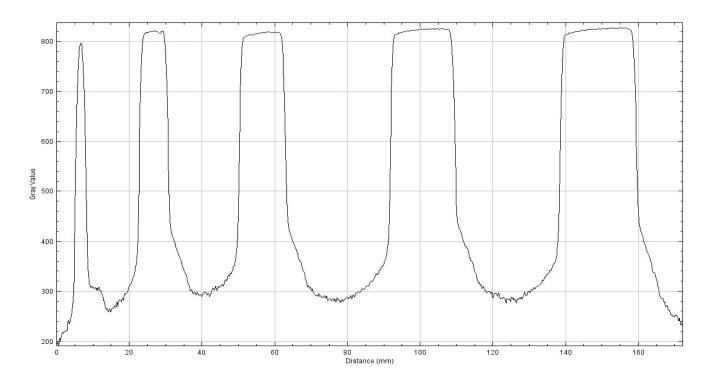
A CR plate was positioned at scanner iso-center and axial images were acquired at selected location. Beam widths were measured at FWHM of the slice profiles.

Detector Configuration (Prescribed Width NxT)	Prescribed Beam Width	Measured Beam Width	Difference	Status (Pass/Fail Criteria)
2i 2x0.625 mm	1.25 mm	2.5 mm	1.3 mm	PASS (≤ 3.0 mm)
4i 4x1.25 mm	5.0 mm	7.6 mm	2.6 mm	PASS (≤ 3.0 mm)
16i 16x0.625 mm	10 mm	12.6 mm	2.6 mm	PASS (≤ 3.0 mm)
4i 4x3.75 mm	15 mm	17.9 mm	2.9 mm	PASS (≤ 4.5 mm)
16i 16x1.25 mm	20 mm	21.2 mm	1.2 mm	PASS (≤ 6.0 mm)

**Conclusion:** Measured beam widths were found to be in good agreement with indicated beam widths.

Measured beam widths have to be within the larger of ± 3 mm or 30% of prescribed total

nominal collimated beam width.



## 6. SLICE THICKNESS ACCURACY EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 1

Technique: 120 kVp, 275 mA, 1.0 sec Rotation Speed, 275 mAs, Axial Mode, Detector Configuration and Slice

Thicknesses as indicated, Standard Reconstruction Algorithm, Large SFOV, 21 cm DFOV, 512x512

Image Matrix.

Axial images were acquired at the center of Module 1 of the ACR CT Accreditation phantom. Slice widths were assessed by counting the visible wires on the two ramps containing wires arranged in 0.5 mm z-axis increments.

Detector Configuration	Prescribed Slice	Measured Slice	Difference
(Prescribed Beam Width NxT)	Width	Width	
16i 16x0.625 mm	0.625 mm	1.0 mm	< 0.5 mm
16i 16x1.25 mm	1.25 mm	1.5 mm	< 0.5 mm
8i 8x2.5 mm	2.50 mm	2.5 mm	0.0 mm
4i 4x3.75 mm	3.75 mm	4.0 mm	< 0.5 mm
4i 16x1.25 mm	5.0 mm	5.0 mm	0.0 mm
2i 4x3.75 mm	7.5 mm	7.5 mm	0.0 mm

Conclusion: Observed slice widths were found to be in good agreement with the nominal slice widths. Slice

widths must be within  $\pm$  1.5 mm of the prescribed slice thickness.

## 7. HIGH CONTRAST SPATIAL RESOLUTION EVALUATION

**Phantom:** ACR CT Accreditation Phantom

**Technique:** Routine Adult Head, Adult Abdomen and HR Chest Protocols

The high contrast resolution insert, Module 4 of the ACR Phantom, contains eight bar patterns representing spatial frequencies corresponding to 4, 5, 6, 7, 8, 9, 10 and 12 lp/cm, respectively.

Protocol	High Contrast Spatial Resolution
Routine Adult Brain Protocol	7 lp/cm
Routine Adult Abdomen protocol	7 lp/cm
HR Chest Protocol	10 lp/cm

**Conclusion:** The limiting high contrast spatial resolution is adequate. The ACR Pass/Fail criteria are 6 lp/cm for

standard resolution head and body protocols and 8 lp/cm for the high resolution chest protocol.

# 8 (a). CONTRAST TO NOISE EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 2 **Technique:** Routine Head and Abdomen Protocols

The low contrast resolution insert, Module 2 of the ACR phantom, contains five different size rod sets with diameters equal to 6 mm, 5 mm, 4 mm, 3 mm, and 2 mm, respectively. The rod sets are considered to be resolved if all four rods of the same size can be clearly visualized.

# Contrast to Noise (CNR) Evaluation:

The low contrast resolution insert, Module 2 of the ACR Phantom, was evaluated using a ROI of about 100 mm<sup>2</sup>. Image noise was represented by the ROI standard deviation of the background area.

Protocol	Rod Insert ROI	Background ROI	Background ROI	CNR
	(H.U.)	(H.U.)	(Std. Dev.)	
Adult Brain Axial 5.0 mm	91.6	85.2	4.0	1.6
Adult Abdomen 2.5 mm	89.8	83.2	5.8	1.1
Pediatric Brain	83.9	77.1	6.5	1.0
Pediatric Abd	81.9	75.1	11.0	0.6

**Conclusion:** Routine Brain and Body protocol contrast to noise ratios were found to be adequate. The CNR

must be greater than 1.0 for the adult Brain and adult Abdomen protocols. CNR must be greater

than 0.7 for Pediatric Brain and greater than 0.4 for Pediatric Abdomen protocol.

# 8 (b). LOW CONTRAST RESOLUTION EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 2

**Technique:** Routine Adult Head and Adult Abdomen Protocols

The low contrast resolution insert, Module 2 of the ACR phantom, contains five different size rod sets with diameters equal to 6 mm, 5 mm, 4 mm, 3 mm, and 2 mm, respectively. The rod sets are considered to be resolved if all four rods of the same size can be clearly visualized .

Protocol	Contrast Level	CTDI <sub>vol</sub> (mGy)	Low Contrast	
			Resolution	
Adult Brain	0.6%	51.29 mGy	4 mm	
Adult Abdomen	0.7%	17.26 mGy	5 mm	
Pediatric Brain (1 Year old)	0.7%	17.24 mGy	5 mm	
Pediatric Abdomen (5 Year old)	0.7%	13.33 mGy	6 mm	

**Conclusion:** The ACR Pass/Fail criteria indicate a resolution of 6 mm diameter rods with both adult abdomen

and adult brain protocols. The scanner Low Contrast Resolution is estimated to better than 4.0

mm @ 0.6 % contrast at a dose of 51 mGy CTDI<sub>vol</sub>.

# 9 (a). CT NUMBER ACCURACY AND LINEARITY EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 1 **Technique:** Routine Brain and Abdomen Protocols

Module 1 of the ACR phantom is used to assess CT number accuracy and linearity. There are five cylinders of different materials including a bone mimicking material ("Bone"), polyethylene, water equivalent material, acrylic and air. Each cylinder, except the water cylinder, has a diameter of 25 mm and a depth of 4 cm. The water cylinder has a diameter of 50 mm and a depth of 4 cm. ROI measurements were performed in each insert with an ROI area of  $\sim 200 \text{ mm}^2$ .

**Technique:** Routine Adult Abdomen Protocol

ACR Phantom Insert	Mean CT Number (HU)	Acceptable CT Number Range		
Polyethylene	-93	-107 HU	to	-84 HU
Water Equivalent	-2.0	-7 HU	to	7 HU
Acrylic	120	110 HU	to	135 HU
Bone	906	850 HU	to	970 HU
Air	-974	-1005 HU	to	-970 HU

Technique: Routine Adult Brain and Pediatric Brain and Abdomen Protocols

PROTOCOL	Adult Brain	Pediatric Brain	Pediatric Abdomen
Polyethylene Insert CT Number (HU)	-93	-103	-104
Water Equivalent Insert CT Number (HU)	-0.1	0.8	-1.2
Acrylic Insert CT Number (HU)	122	117	113
Bone Insert CT Number (HU)	970	1103	1028
Air CT Number (HU)	-974	-973	-971

Conclusion: CT number calibration accuracy is adequate. Mean CT number of tested inserts with the

Abdomen Protocol are within ACR recommended ranges.

# 9 (b). CT NUMBER CONTRAST SCALE EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 1

**Technique:** Routine Adult Brain and Adult Abdomen Protocols

CT number contrast scale was evaluated using the Water and Acrylic inserts in Module 1 of the ACR Phantom. Acrylic/Water CT number contrast scale was represented by the difference in Acrylic and Water CT numbers.

PROTOCOL	Acrylic CT Number	Water CT Number	Contrast Scale	
Routine Adult Brain protocol	120.0	-2.0	122	HU
Routine Adult Abdomen protocol	122.4	-0.1	123	HU

**Conclusion:** Contrast scale is adequate. The acrylic and water CT number difference should be within  $120 \pm 12$ 

HU.

# 9 (c). CT NUMBER DEPENDENCE ON SLICE THICKNESS EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 1

**Technique:** Adult Abdomen equivalent axial protocol at 120 kVp, 275 mA, 1.0 sec Rotation Time, Small SFOV,

21 cm DFOV, Standard Body Algorithm, slice thicknesses as indicated and ROI areas of ~ 200

mm<sup>2</sup>.

Slice Thickness	Mean CT Number (HU)	Acceptable CT Number Range		ber Range
0.625 mm	-2.2	-7 HU	to	7 HU
1.25 mm	-2.4	-7 HU	to	7 HU
2.5 mm	-2.4	-7 HU	to	7 HU
3.75 mm	-1.3	-7 HU	to	7 HU
5.0 mm	-2.1	-7 HU	to	7 HU
7.5 mm	-1.5	-7 HU	to	7 HU

**Conclusion:** CT number dependence on slice thickness is adequate. Mean CT numbers should be within the

ACR recommended range of  $\pm$  7 HU, and preferably within  $\pm$  5 HU.

# 9 (d). CT NUMBER DEPENDENCE ON kVp EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 1

**Technique:** Routine Adult Abdomen equivalent protocol in axial mode 2.5 mm Slice Thickness, 275 mA, 1.0

sec Rotation Time, and kVp values as indicated with ROI areas of ~ 200 mm<sup>2</sup>.

kVp	Mean CT Number (HU)	Acceptable CT Number Range		ber Range
80	-2.0	-7 HU	to	7 HU
100	-3.4	-7 HU	to	7 HU
120	-2.6	-7 HU	to	7 HU
140	-2.6	-7 HU	to	7 HU

**Conclusion:** CT number dependence on kVp is adequate at all kVp settings. Mean CT numbers should be

within the ACR recommended range of  $\pm$  7 HU, and preferably within  $\pm$  5 HU.

# 9 (e). IMAGE UNIFORMITY EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 3

**Technique:** Routine Adult Abdomen Protocol

The uniformity section insert, Module 3 of the ACR phantom, contains Teflon beads embedded in a uniform water equivalent background. ROI measurements were performed at the center and periphery of the phantom. Area of ROI used was ~ 400 mm2. Image spatial uniformity was depicted by the edge-to-center mean CT number differences.

ACR Phantom	Location	Mean ROI CT	ROI Standard	Difference Center to
		Number (H.U.)	Deviation (H.U.)	Edge ROI (H.U.)
ROI ~ 400 mm <sup>2</sup>	Center	-1.0	7.2	
	3 O'clock	-2.1		1.1
	6 O'clock	-1.8		0.8
	9 O'clock	-1.5		0.5
	12 O'clock	-2.4		1.4

**Conclusion:** 

Mean CT number and image spatial uniformity is adequate. The measured mean CT numbers should be in the range of  $0\pm7$  Hounsfield Units (HU) and preferably within  $0\pm5$  HU. Image spatial uniformity, depicted by the edge-to-center mean CT number differences is also within recommended limits. Edge-to-center mean CT number differences must be less than 5 HU for all four edge positions.

## **10. ARTIFACT EVALUATION**

**Phantom:** ACR CT Accreditation and CTDI Dose Phantoms

**Technique:** Routine Adult Brain and Adult Abdomen Protocols

With all graphics turned off and with reduced room lighting, images were viewed for artifacts, such as ring or streak artifacts.

**Conclusion:** No significant ring, streak or other equipment related artifacts were noted.

## 11. CT DOSIMETRY EVALUATION

# A. CT SCANNER INDICATED COMPUTED TOMOGRAPHY DOSE INDEX (CTDI<sub>VOL</sub>) EVALUATION

**Phantom:** 16 cm CTDI Acrylic Head and 32 cm CTDI Acrylic Body Phantom

**Dosimeter Used:** Radcal Accu-Pro Model 9096 S/N 96-0544

**Ion Chamber:** Radcal 10X6-3CT Ion Chamber

**Technique:** Axial Brain and Abdomen Protocols

## Weighted CTDI<sub>w.100</sub> Dose Measurements using CTDI Dose Phantoms:

Scan Protocols	kVp	mA	Scan	SFOV	Scan	Indicated	Measured	Percent
			Time	(cm)	Type	CTDI <sub>vol</sub>	CTDI <sub>w</sub>	Difference
			(sec)			(mGy)	(mGy)	
Adult Brain	120	150	2.0	Head	Axial	51.29	51.22	0%
(16x1.25 mm)				(25 cm)		(Head16)		
Adult Abdomen	120	275	1.0	Large	Axial	23.74	23.81	0%
(16x1.25 mm)				(50 cm)		(Body32)		
Pediatric Brain	100	190	0.8	Ped Head	Axial	17.24	16.08	-7%
(16x1.25 mm)				(25 cm)		(Head16)		
Pediatric Abdomen	100	200	0.8	Small	Axial	18.33	17.59	-4%
(16x1.25 mm)				(25 cm)		(Head 16)		

**CONCLUSION:** Measured CTDI<sub>w</sub> values were found to be consistent with indicated CTDI<sub>vol</sub> values.

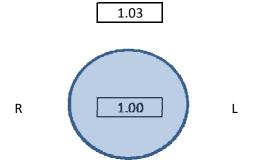
Percent differences were within an acceptable range of ± 20.0%.

## **RADIATION DOSE UNIFORMITY\***

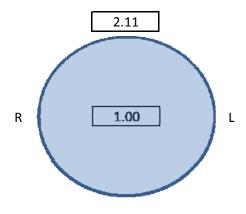
\*Note: Phantom surface dose factors normalized relative to the value at the center location

**Technique:** 120 kVp Adult Techniques as indicated in table above

## 16 cm CTDI Head Dose Phantom



## 32 cm CTDI Body Dose Phantom



# 11. CT DOSIMETRY EVALUATION (Continued)

#### B. PATIENT DOSE EVALUATION FOR REPRESENTATIVE CT EXAMINATIONS

**Phantom:** 16 cm CTDI Acrylic Head and 32 cm CTDI Acrylic Body Phantom

**Technique:** Routine Brain and Abdomen Protocols

**Correspondence of Measured and Indicated CTDI**<sub>vol</sub> Doses for Select Clinical Protocols:

Protocols	Measured CTDI <sub>vol</sub> (mGy)	Indicated CTDI <sub>vol</sub> (mGy)	Reference CTDI Dose Phantom	Percent Difference
Adult Brain	51.22 mGy	51.29 mGy	Head 16 cm	0%
Adult Abdomen	17.31 mGy	17.26 mGy	Body 32 cm	0%
Pediatric Brain	16.08 mGy	17.24 mGy	Head 16 cm	-7%
Pediatric Abdomen*	12.79 mGy	13.33 mGy	Head 16 cm	-4%

**CONCLUSION:** Measured CTDI<sub>vol</sub> dose values were found to be consistent with indicated CTDI<sub>vol</sub> values.

Percent differences were within an acceptable range of  $\pm$  20%.

#### C. PATIENT DOSE EVALUATION FOR REPRESENTATIVE CT EXAMINATIONS

#### **Effective Dose Estimates for Select Clinical Protocols**

Protocols	Measured CTDI <sub>vol</sub> (mGy)	Scan Length	Dose Length Product DLP (mGy.cm)	Effective Dose (mSv)
Adult Brain	51.22 mGy	17.5 cm	896 mGy.cm	1.9 mSv
Adult Abdomen (SSDE**)	17.74 mGy	25.0 cm	444 mGy.cm	6.7 mSv
Pediatric Brain	16.08 mGy	12.0 cm	193 mGy.cm	1.3 mSv
Ped Abdomen (SSDE**)	11.72 mGy	15.0 cm	176 mGy.cm	3.5 mSv

**CONCLUSION:** CTDI<sub>vol</sub> dose values and Effective Dose estimates are well within the ACR recommended

limits. Attached, please find dose calculator spreadsheets for further details. Measured CTDI<sub>vol</sub> values should be less than the ACR Pass/Fail Criteria tabulated below, and preferably

less than the ACR Reference Dose Levels.

## ACR CTDI<sub>vol</sub> Pass/Fail Criteria and CT Dose Reference Levels

CT Examination	ACR Pass/Fail Criteria CTDI <sub>vol</sub> (mGy)	ACR Reference Levels CTDI <sub>vol</sub> (mGy)
Adult Head	80 mGy	75 mGy
Adult Abdomen	30 mGy	25 mGy
Pediatric Head (1 year old)	40 mGy	35 mGy
Pediatric Abdomen (40-50 lb) - 16 cm Diameter CTDI Phantom	20 mGy	15 mGy
Pediatric Abdomen (40-50 lb) - 32 cm Diameter CTDI Phantom	10 mGy	7.5 mGy

<sup>\*</sup>Note: Pediatric Abdomen dose measured using the "Small" SFOV and the small (16 cm Diameter) CTDI Phantom.

<sup>\*\*</sup>SSDE: Size Specific Dose Estimate

# 12 (a). ACQUISITION DISPLAY DEVICE EVALUATION

**Luminance Meter Make/Model:** RaySafe X2 Photometer

## Acquisition display devices were evaluated using a standard SMPTE test pattern:

- 1. The 5% and the 95% square contrast patterns were properly resolved and visualized.
- 2. Each gray-level step from 0% to 100% was uniform and distinct from the adjacent step.
- 3. The borders and lines of the SMPTE pattern were straight.
- 4. No spatial distortions or misalignments were noted in the grids across the screen.
- 5. Alphanumeric characters looked sharp and focused.
- 6. The high contrast line-pair resolution patterns in the center and corners of the display area were linear, properly resolved and adequately visualized without any magnification.
- 7. No streaking was noted in and around the white and black rectangular patterns.

The overall appearance of the SMPTE pattern was found to be adequate.

The soft copy display monitor resolution and spatial accuracy was found to be adequate.

No significant distortions or any kind of non-linearities were noted in any of the target patterns.

Monitor	Minimum Luminance	Maximum Luminance	% Luminance
NEC MultiSync LCD 1980SXi	(Black Level)	(White Level)	Non-Uniformity
Acquisition Workstation Display	0.15 cd/m <sup>2</sup>	122 cd/m <sup>2</sup>	14%

The minimum luminance (Black Level) should be less than 1.2 cd/m<sup>2</sup>.

The maximum luminance (White Level) should be greater than or equal 100 cd/ $m^2$  for diagnostic workstations. The display luminance uniformity is considered adequate if percent luminance non-uniformity is within  $\pm$  15%.

**CONCLUSION:** The display monitor minimum & maximum luminances and uniformity were found to be adequate.

# 12 (b). SPATIAL DISTORTION EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 3

**Technique:** Routine Adult Abdomen Protocol

Spatial distortion and distance measurement accuracy was evaluated by measuring the known dimensions of the ACR phantom and set distance between the Teflon BB's in Module 3.

## A. Distance Gauge Check:

Orientation of BB's	Actual Distance Between BB's	Scanner Measured Distance	Percent Difference
45°	10.0 cm	10.0 cm	0.0%

### B. Aspect Ratio of Video Monitor and Imager (if available):

ACR Phantom	Aspect Ratio
Ratio of Horizontal to Vertical Dimensions of Circular Phantom Object	1.00
Ratio of Horizontal to Vertical Dimensions of Object on the Monitor	1.00
Ratio of Horizontal to Vertical Dimensions of Object on Film	N/A

**CONCLUSION:** The scanner distance measurement accuracy is adequate. There are no significant spatial

distortion of the image on the monitors.

## 13. RADIATION SAFETY EVALUATION

## A. Visual Inspection

A visual safety inspection of the CT Trailer and surroundings was conducted. No unsafe conditions were noted.

## B. Audible and Visual Warning Signs

System audible and visual warning signs are functional and performing adequately. Dose Notification and Dose Alert features are activated and functioning properly.

# C. Posting Requirements

CT scanner room was appropriately posted with a "Caution X-Ray" warning sign.

# 14. TECHNOLOGIST QUALITY CONTROL PROGRAM

A. Technologist QC program is well established. Daily QC procedures are properly performed and documented on the days the scanner is used. Recommend documenting the visual checklist and display monitor QC tests also on a monthly basis.

<b>Quality Control Procedures</b>	Responsible	Frequency	STATUS
	Individual		
1. Water CT Number Accuracy Eval	CT Technologist	Daily	PASS
2. Image Noise Evaluation	CT Technologist	Daily	PASS
3. Artifact Evaluation	CT Technologist	Daily	PASS
4. Visual Checklist	CT Technologist	Monthly	PASS
5. Dry Laser QC	CT Technologist	N/A	N/A
6. Acquisition Display QC	CT Technologist	Monthly	PASS

B. Preventive maintenance program is well established. Regular PMs are periodically performed and documented by qualified field service engineers.

IMPORTANT NOTE: This Excel Workbook contains formulae essential to accurate reporting of dose for ACR CT Accreditation. It is intended to be used with both Windows and Mac operating systems. Please note, ANY alteration of the formulae will very likely result in errors of reported data, and could adversely affect our accreditation results. You must enter accurate data from this workbook into the ACRedit online testing package. Please check the results from this workbook against the results shown in the ACRedit database online testing package before submission.

Dose Calculator Spreadsheet (Exposure)	CTAP ID Number	
Radiation Dosimetry (Adult Head)		

CTDI Head Phantom (16-cm diameter PMMA Phantom)	Measured	Calculated	
kV	120		
mA	150		
Exposure time per rotation (s)	2		
# data channels used (N) <sup>1</sup>	16		
Z-axis collimation (T) <sup>1</sup>	1.25		
Axial (A): Table Increment (mm) = (I) <sup>1</sup> OR	20		
Helical (H):Table Speed (mm/rot) = (I) <sup>1</sup>	20		
Active Chamber length (mm)	100		
Chamber correction factor	1		
Center			
Measurement 1 (mR)	1158		
Measurement 2 (mR)	1158		
Measurement 3 (mR)	1158		
Average of above 3 measurements (mR)		1158	
Head CTDI at isocenter in phantom (mGy)		50.4	
12 o'clock position			
Measurement 1 (mR)	1188		
Measurement 2 (mR)	1188		
Measurement 3 (mR)	1186		
Average of above 3 measurements (mR)		1187	
Head CTDI at 12 o'clock position in phantom (mGy)		51.6	
		54.22	
CTDIw (mGy)	d Drotocal from Table	51.22	
Clinical exam dose estimates (using measured CTDIw and site's Adult Head	=CTDIw*N*T/I	51.22	
CTDIvol (mGy)	=CIDIW*N*1/I	51.22	
CTDIvol reported by scanner (mGy) for the protocol entered in the phantom site scanning data form (using 16-cm diameter PMMA phantom)	51.29		
Percent difference between calculated CTDIvol and CTDIvol reported by scanner		0%	
Dose Notification Value (mGy) as described in XR-29 (if applicable)			
DLP (mGy-cm)	=CTDIvol*17.5	896	

<sup>&</sup>lt;sup>1</sup>See definitions in the CT Accreditation Testing Instructions.

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IMPORTANT NOTE: This Excel Workbook contains formulae essential to accurate reporting of dose for ACR CT Accreditation. It is intended to be used with both Windows and Mac operating systems. Please note, ANY alteration of the formulae will very likely result in errors of reported data, and could adversely affect our accreditation results. You must enter accurate data from this workbook into the ACRedit online testing package. Please check the results from this workbook against the results shown in the ACRedit database online testing package before submission.

# **Dose Calculator Spreadsheet (Exposure)**

**CTAP ID Number** 

# Radiation Dosimetry (Adult Abdomen)

CTDI Body Phantom (32-cm diameter PMMA Phantom)	Measured	Calculated
kV	120	
mA	275	
Exposure time per rotation (s)	1	
# data channels used (N) <sup>1</sup>	16	
Z-axis collimation (T) <sup>1</sup>	1.25	
Axial (A): Table Increment (mm) = $(I)^1$ OR	27.5	
Helical (H):Table Speed (mm/rot) = (I) <sup>1</sup>	27.5	
Active Chamber length (mm)	100	
Chamber correction factor	1	
Center		
Measurement 1 (mR)	314.8	
Measurement 2 (mR)	315.2	
Measurement 3 (mR)	314.3	
Average of above 3 measurements (mR)		314.8
Body CTDI at isocenter in phantom (mGy)		13.7
12 o'clock position		
Measurement 1 (mR)	663.0	
Measurement 2 (mR)	663.5	
Measurement 3 (mR)	663.6	
Average of above 3 measurements (mR)		663.4
Body CTDI at12 o'clock position in phantom (mGy)		28.9
CTDIw (mGy)		23.81
Clinical exam dose estimates (using measured CTDIw and site's Adult Abdomer	Protocol from Table 1)	
CTDIvol (mGy)	=CTDIw*N*T/I	17.31
CTDIvol reported by scanner (mGy) for the protocol entered in the phantom	17.26	
site scanning data form (using 32-cm diameter PMMA phantom)	17.26	
Percent difference between calculated CTDIvol and CTDIvol reported by		0%
scanner		U%
Dose Notification Value (mGy) as described in XR-29 (if applicable)	35	
DLP (mGy-cm)	=CTDIvol*25	433
SSDE for 35 cm water equivalent diameter (mGy)	=SSDE(35 cm)	17.74

<sup>&</sup>lt;sup>1</sup>See definitions in the CT Accreditation Testing Instructions.

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# Dose Calculator Spreadsheet (Exposure) CTAP ID Number Radiation Dosimetry (Pediatric Head, 1 year old)

#### CTDI Head Phantom (16-cm diameter PMMA Phantom) Measured Calculated k۷ 100 mΑ 190 Exposure time per rotation (s) 0.8 16 # data channels *used* (N)<sup>1</sup> Z-axis collimation (T)<sup>1</sup> 1.25 Axial (A): Table Increment (mm) = (I)<sup>1</sup> 20 Helical (H): Table Speed (mm/rot) = $(I)^1$ Active Chamber length (mm) 100 Chamber correction factor 1 Center 333.3 Measurement 1 (mR) Measurement 2 (mR) 334.3 Measurement 3 (mR) 334.8 Average of above 3 measurements (mR) 334.1 Head CTDI at isocenter in phantom (mGy) 14.5 12 o'clock position Measurement 1 (mR) 385.4 Measurement 2 (mR) 389.2 Measurement 3 (mR) 388.0 Average of above 3 measurements (mR) 387.5 Head CTDI at 12 o'clock position in phantom (mGy) 16.9 CTDIw (mGv) 16.08 Clinical exam dose estimates (using measured CTDIw and site's Pediatric Head (1 year old) Protocol from Table 1) =CTDIw\*N\*T/I CTDIvol (mGv) 16.08 CTDIvol reported by scanner (mGy) for the protocol entered in the phantom 17.24

Dose Notification value as desciribed in XR-29 (if applicable)

scanner

DLP (mGy-cm)

site scanning data form (using 16-cm diameter PMMA phantom)

Percent difference between calculated CTDIvol and CTDIvol reported by

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193

=CTDIvol\*12

<sup>&</sup>lt;sup>1</sup>See definitions in the CT Accreditation Testing Instructions.

IMPORTANT NOTE: This Excel Workbook contains formulae essential to accurate reporting of dose for ACR CT Accreditation. It is intended to be used with both Windows and Mac operating systems. Please note, ANY alteration of the formulae will very likely result in errors of reported data, and could adversely affect our accreditation results. You must enter accurate data from this workbook into the ACRedit online testing package. Please check the results from this workbook against the results shown in the ACRedit database online testing package before submission.

Dose	Calculator	<b>Spreadsheet</b>	(Exposure)	
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CTAP ID Number

# Radiation Dosimetry (Ped Abdomen, 40-50 lb)

Note: For pediatric abdomen (40-50 lb.)protocols, some CT scanners report CTDIvol using the 16 cm phantom, while others use the 32 cm phantom. The physicist should use the phantom (16 or 32 cm ) that is used by the scanner to report CTDIvol.

CTDI Phantom (16 or 32 cm diameter PMMA Phantom)	Measured	Calculated
Size of phantom the scanner uses to report CTDIvol for routine pediatric	16 cm	
abdomen protocol (40-50 lb.)		
kV	100	
mA	200	
Exposure time per rotation (s)	0.8	
# data channels used (N) <sup>1</sup>	16	
Z-axis collimation (T) <sup>1</sup>	1.25	
Axial (A): Table Increment (mm) = $(I)^1$ OR	27.5	
Helical (H):Table Speed (mm/rot) = (I) <sup>1</sup>	27.3	
Active Chamber length (mm)	100	
Chamber correction factor	1	
Center		
Measurement 1 (mR)	366.5	
Measurement 2 (mR)	366.5	
Measurement 3 (mR)	365.2	
Average of above 3 measurements (mR)		366.1
Ped Body CTDI at isocenter in phantom (mGy)		15.9
12 o'clock position		
Measurement 1 (mR)	423.4	
Measurement 2 (mR)	423.4	
Measurement 3 (mR)	423.4	
Average of above 3 measurements (mR)		423.4
Ped Body CTDI at12 o'clock position in phantom (mGy)		18.4
CTDIw (mGy)		17.59
Clinical exam dose estimates (using measured CTDIw and site's Pediatric Abdo	men (40-50 lb.) Protocol	from Table 1)
CTDIvol (mGy)	=CTDIw*N*T/I	12.79
CTDIvol reported by scanner (mGy) for the protocol entered in the phantom	13.33	
site scanning data form	15.55	
Percent difference between calculated CTDIvol and CTDIvol reported by		-4%
scanner  Description Value and described by VP 20 (if any limit)		
Dose Notification Value as described in XR-29 (if applicable)		100
DLP (mGy-cm)	=CTDIvol*15	192
SSDE for 18.5 cm water equivalent diameter (mGy)	=SSDE(18.5 cm)	11.7

<sup>&</sup>lt;sup>1</sup>See definitions in the CT Accreditation Testing Instructions.

